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#### Sviluppo di nuovi dispositivi biotecnologici per la validazione di nuovi approcci terapeutici

#### Prof. Giovanni Vozzi

Biofabrication Group Research Center E. Piaggio and Department of Ingegneria dell'Informazione CIRHTA Centro per lo Studio e la Ricerca in Health Technology Assessment University of Pisa, Italy

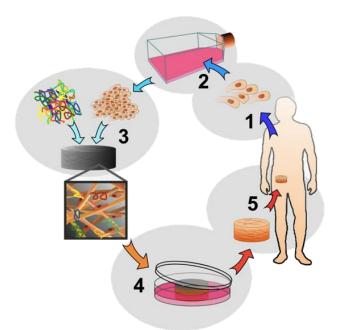






## **Regenerative medicine**

the application of tissue science, tissue engineering, and related biological and engineering principles that restore the structure and function of damaged tissues and organs



U.S. department of health and human services, 2006: A New Vision - A Future for Regenerative Medicine,

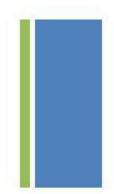
# Living tissues Multiscale and multimaterial structure bone retina **Material** Function blood vesses

Vozzi G and Ahluwalia A. Microfabrication for tissue engineering: rethinking the cells-on-a scaffold approach, J Mat Chem 17 (13), 1248-1254









### **Biofabrication of human organs**

Topologic

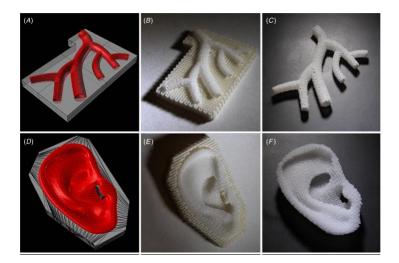
**Mechanical** 

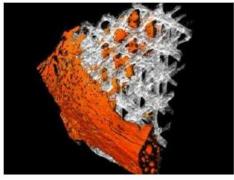
**Biochemical** 

- Mimicking the stimuli that drive growth and functions of cells in living tissues
- Tailor the scaffold properties using combinations of advanced fabrication technologies
- Allowing the tissue maturation into appropriate bioreactors

### What is a scaffold?

Scaffold is a **temporary** 3D polymeric structure that **mimics** the mechanical, structural, and **biochemical** properties of the extracellular matrix (ECM) of natural tissue supporting 3D tissue growth

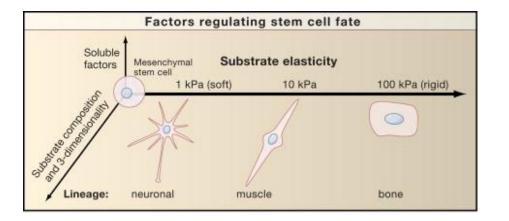


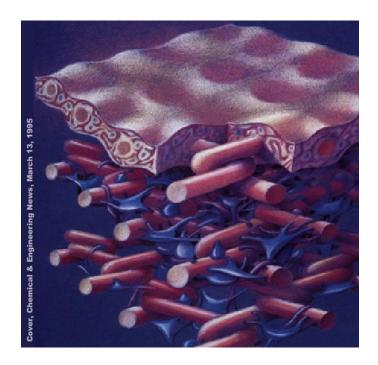




### **Biochemical stimulus**

- Synthetic biomaterials with ligands
- Natural biomaterials
- Decellularized Tissue





Even-Ram s et al, Matrix Control of Stem Cell Fate, Cell. Volume 126, Issue 4, 25 August 2006, Pages 645–647

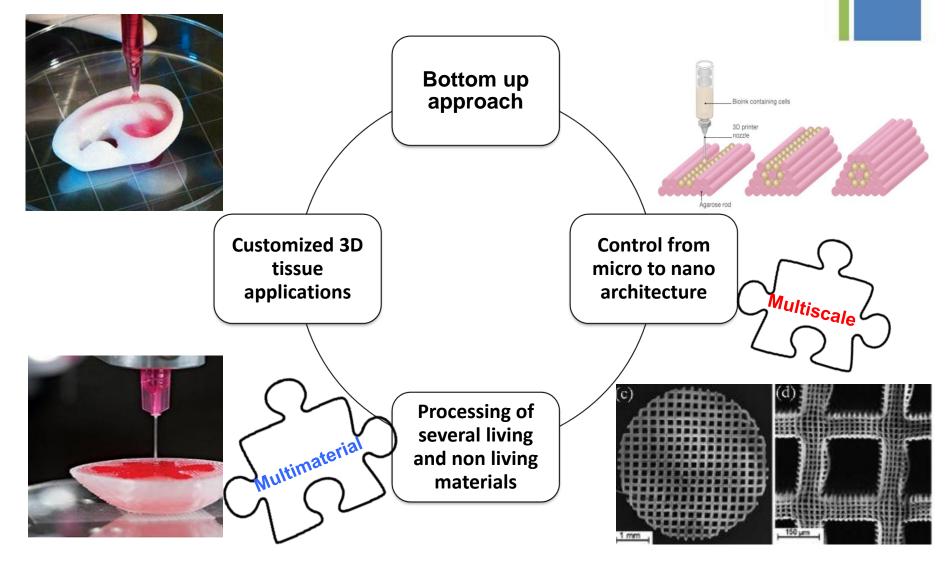


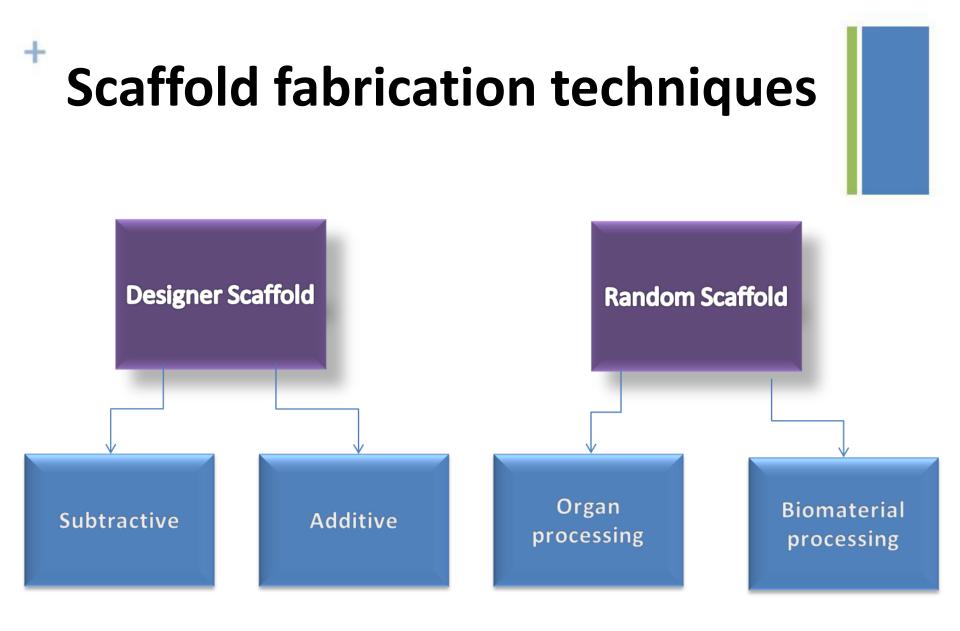
## **Biochemical stimulus**

Biomateri al	Reproducibi lity	Processabili ty	Biochemical features	Mechanical feature
Synthetic	$\checkmark$	$\checkmark$	Х	Х
Natural	Х	Х	V	$\checkmark$
Decellulariz ed	Х	Х	V	V

#### There is no one ideal material for tissue model....

# Why Rapid Prototyping in organ/tissue regeneration ?





# Scaffold fabrication techniques

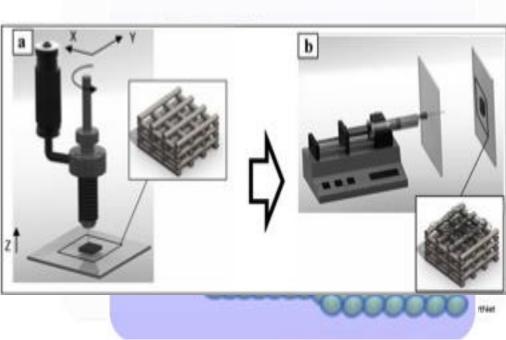
Three main groups:

○ laser systems

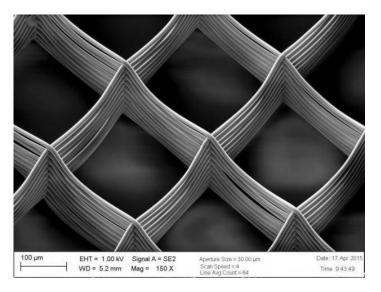
 $\circ$  nozzle based systen

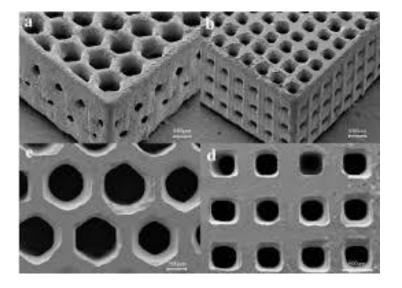
 $\circ$  extrusion systems

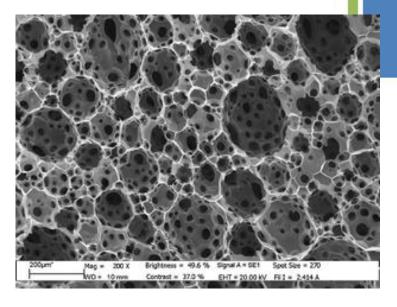
o hybrid systems



### Scaffolds

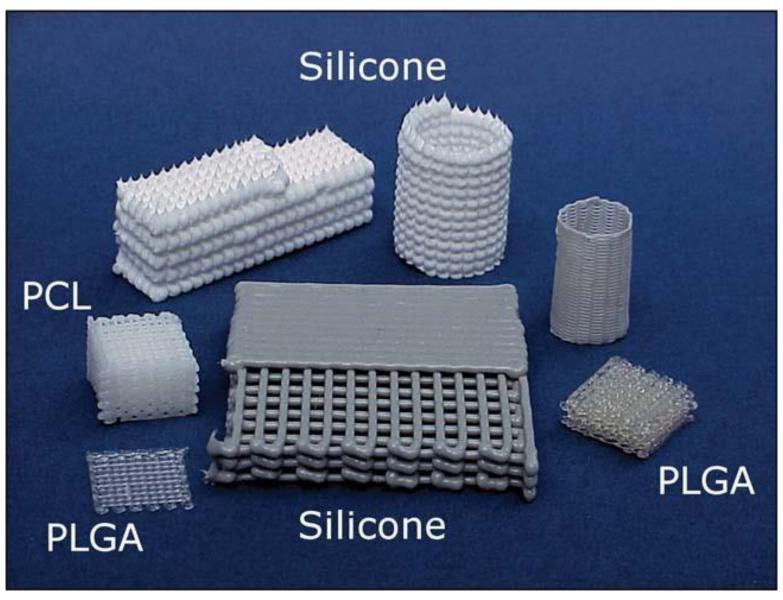






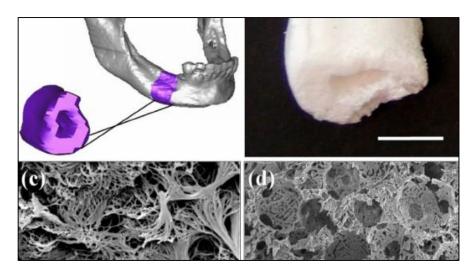


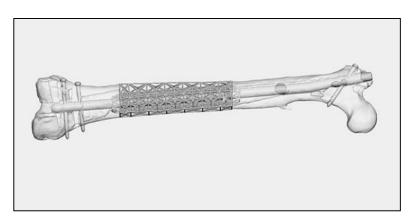
### Scaffolds



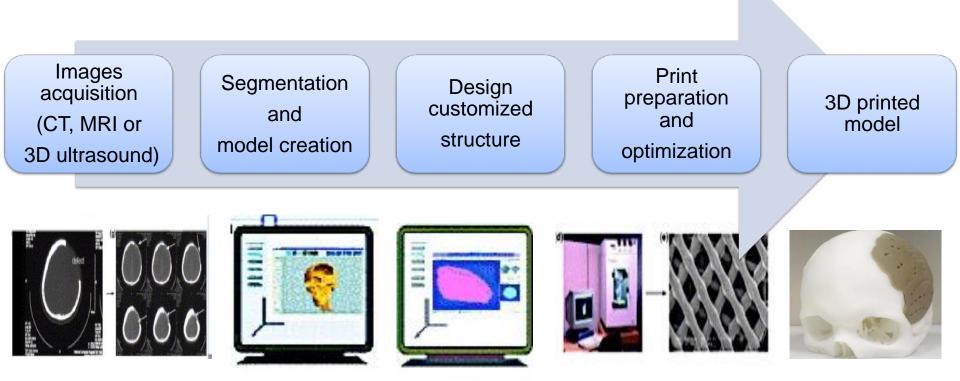
### **RP: towards patient specific scaffold**

RP creates **patient-specfic** solutions that perfectly mimic the physical shape to potentially restore the original functionality of a tissue





### RP workflow : from patient images to the 3D model

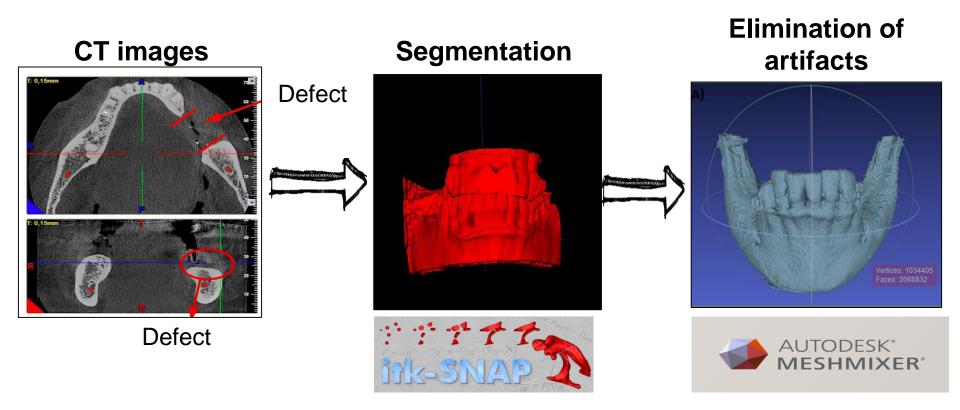




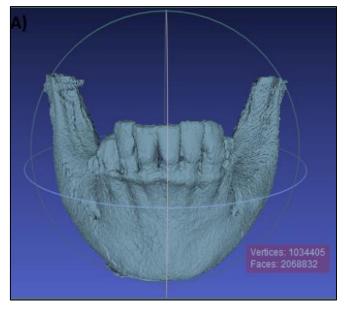
Computer aided design (CAD) software are the key of this workflow !



### **Segmentation procedure**



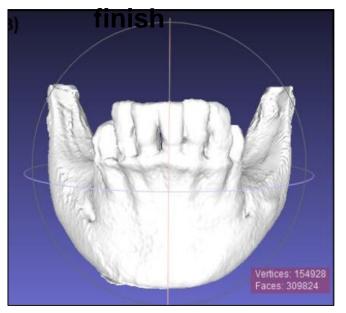






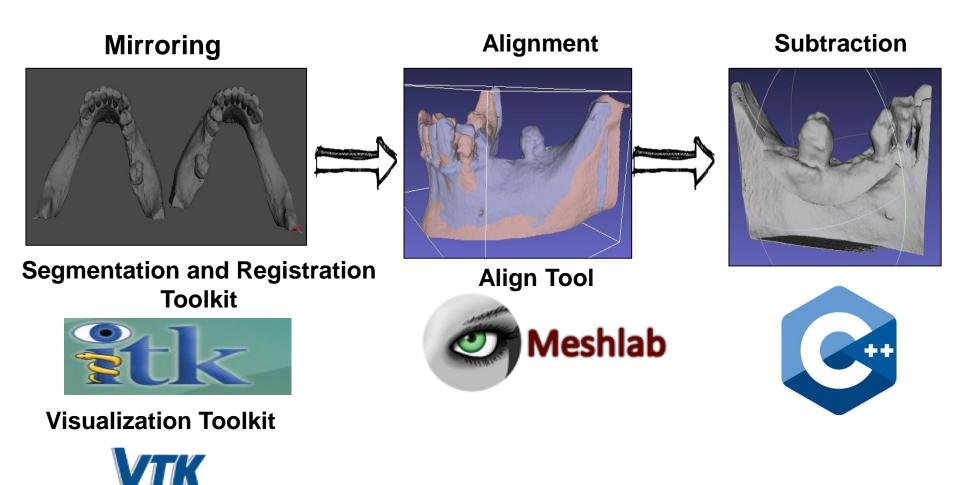


#### surface



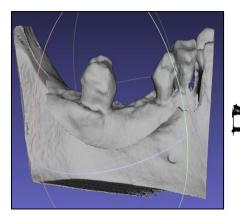


### **Identification of defect**

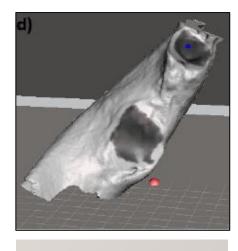


### **Preparing to print**

#### Segmented model

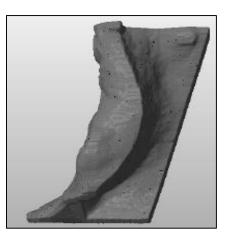


#### Model optimization

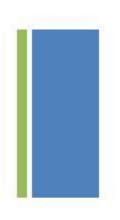




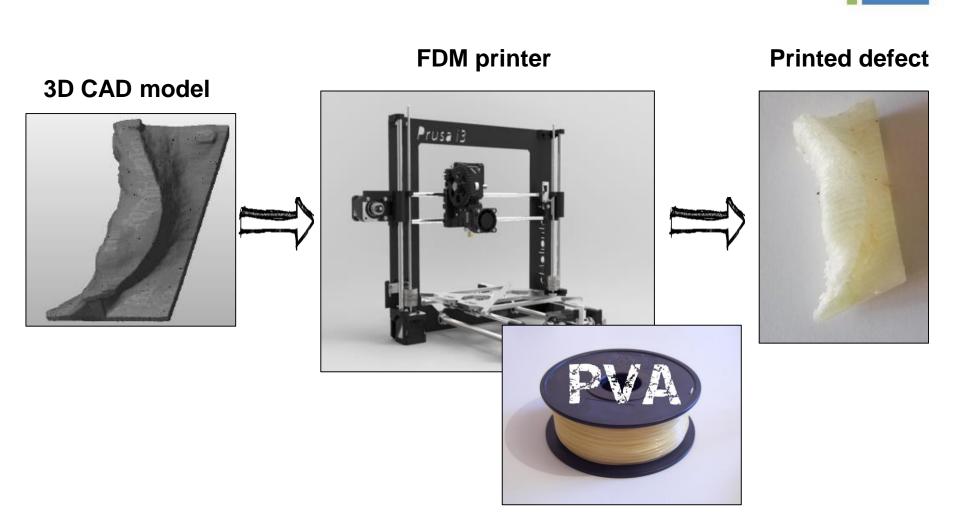
#### Slicing



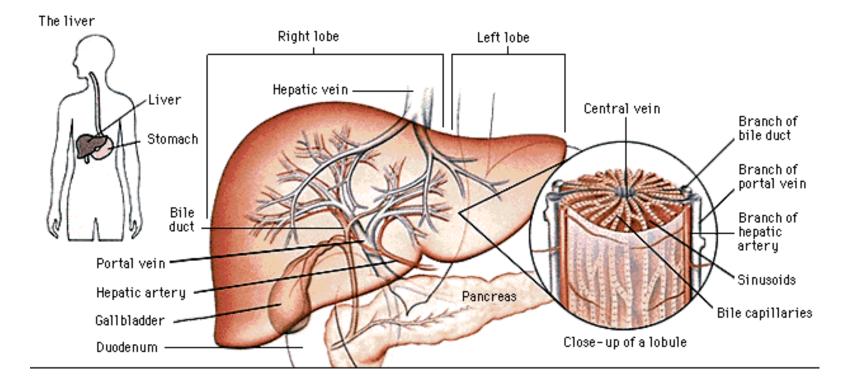




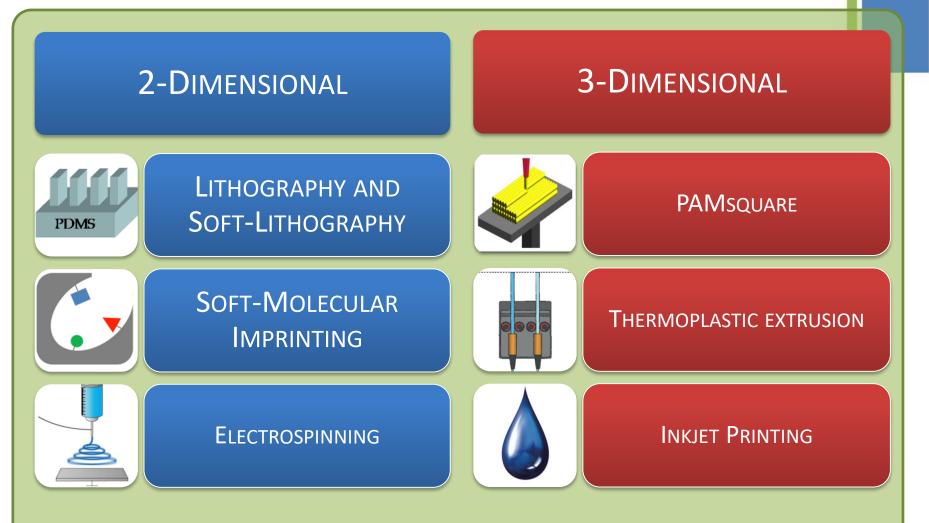
### **Printing the model**



### Living tissues: multiscale e multimaterial



# **Multimaterial processing**



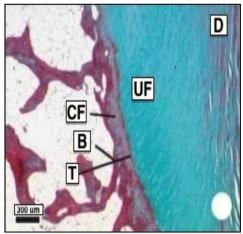
COMBINATION OF 2D AND 3D TECHNOLOGIES

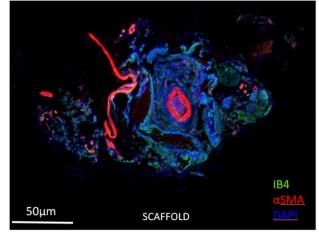
# Multimaterial biofabrication for tiisue model

- Human skin
- Bone ligament interface
- Angiogenesis
- Retinal Pigment Epithelium of human eye





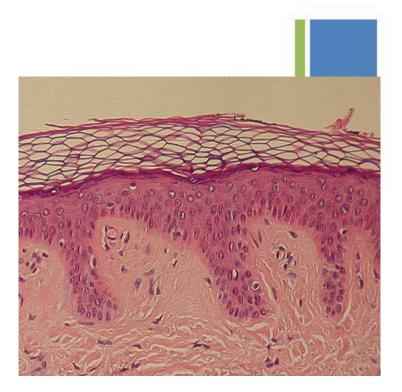




#### +

Aim of the work

- Validate keratin from chicken feathers as biomaterial
- Propose an added-value products from animal waste
- In vitro model of human skin

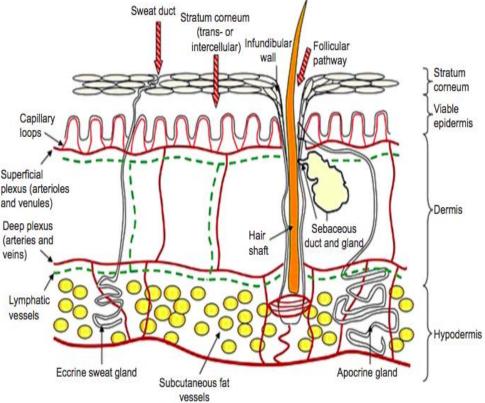


# IN VITRO MODEL OF HUMAN SKIN

De Maria C. et al. *Hydroxylated Keratin from chicken feather as novel substrate for in vitro tissue model fabrication.* Biofabrication 2017 – Beijing, China, Oct 15-18 2017

# Skin in vitro model

- Applications
  - Topical formulation development
  - Skin irritancy and toxicity
  - Skin disease model
- Requirements
  - Availability (storage)
  - easiness of use
  - cost
  - limitations (functions, including mechanical properties and ethics)

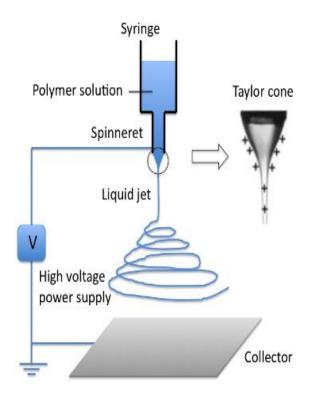


# Skin model: state of the art

Table I Skin models

Model	Advantages	Disadvantages	
Human skin			
In vivo	Gold standard	Often precluded for ethical and practical reasons	
Ex vivo skin	Best surrogate for in vivo humans	Not readily available, variability	
Animal skin	_		
In vivo	Reasonably easy to obtain animals, can be scaled up to humans, hairless species available	Pigs: similar barrier to humans, but difficult to handle Rodents: different barrier properties from humans	
In vivo chimeric model	Human skin xenografts on mice allows testing on living human skin	Technically difficult	
Ex vivo skin	Easy to obtain	Different barrier properties, variability	
Artificial membranes			
Simple polymeric models	Useful for studying basic diffusion mechanisms, consistent and homogenous	Not representative of human skin	
Lipid-based models	Useful for screening	Not representative of human skin	
Reconstructed skin models	-		
Reconstructed human epidermis	Built-in barrier properties	Usually more permeable than human skin	
Living skin equivalents Can be engineered to include a range of normal or disease features		Usually more permeable than human skin	

### Keratin-based electrospun films



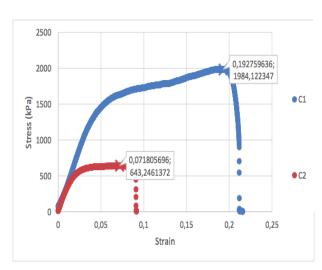




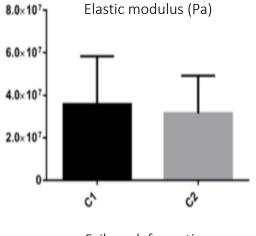
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### **Mechanical characterization**

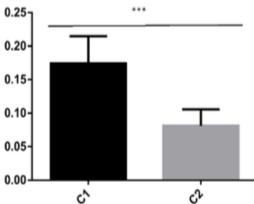
Composition	Distance (cm)	Flow (ml/h)	Voltage(kV)	TIme (h)
2:1	20	1	30	2
1:1	20	1	30	2

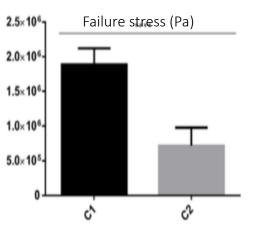


The elastic modulus of electrospun structures is in the range [30-70] MPa, similar to skin

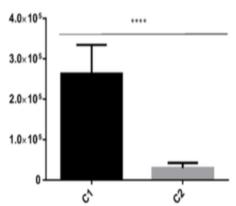


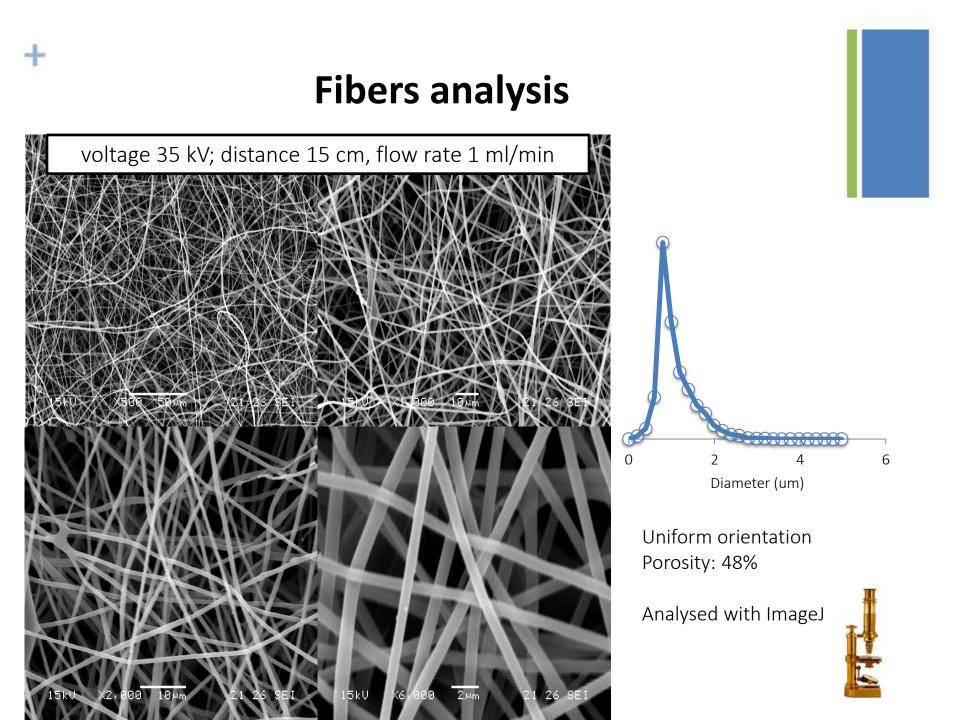






Tenacity (J/m<sup>3</sup>)



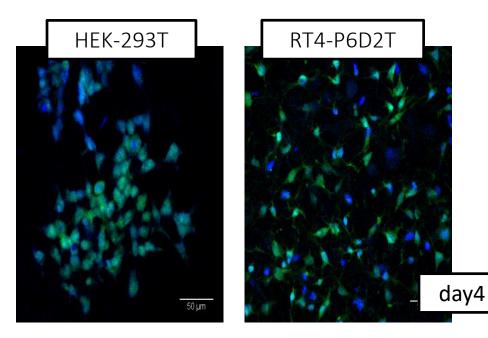


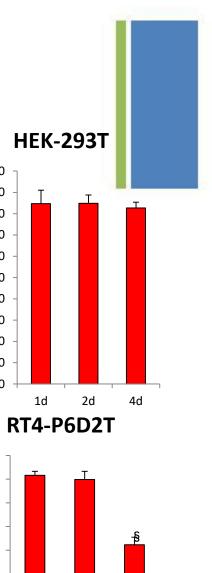
# **Biological validation**

- Tests were conducted on spuns obtained with the following parameters: voltage 35 kV; distance 15 cm, flow rate 1 ml/min
- Human epithelial HEK-293T cells,
- Rat neuronal RT4-P6D2T cells
- Density 20000 cells/well in 12well plate on keratin/gelatin electrospun
- Cultured in DMEM-10%FBS (Invitrogen) for 1, 2 and 4 days.

#### Cell vitality

 CellTracker ™Green CMFDA (5µM in PBS, Invitrogen) was added for 1,5 hours before fixation





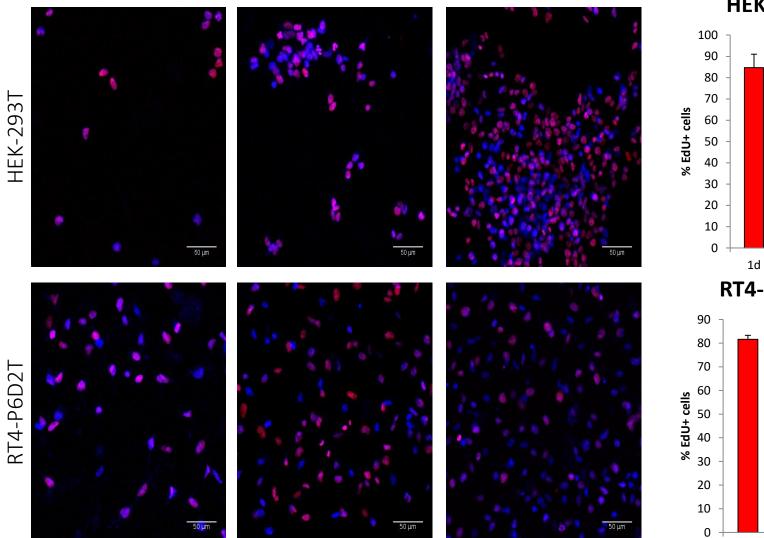
1d

4d

2d

4d

### **EdU Proliferation assay**



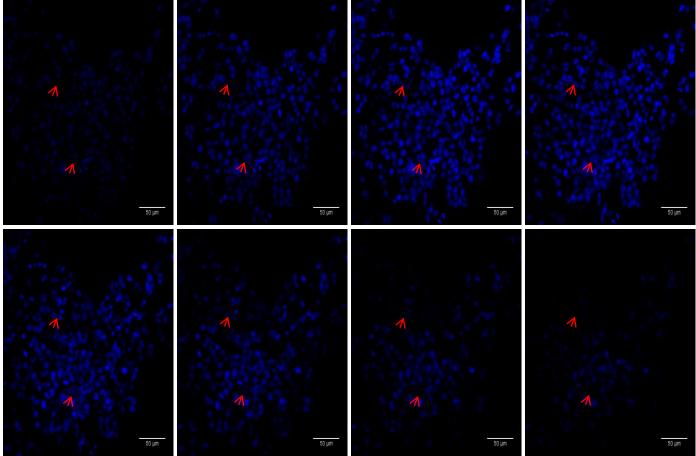
2d

1d

# Cell penetration into the scaffold

• HEK-293T at day4

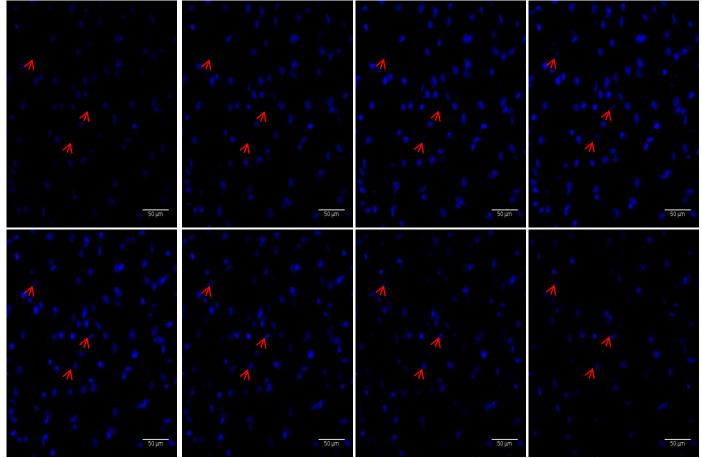
t



Hoechst 33258 (Sigma Aldrich) was used as nuclear counterstain

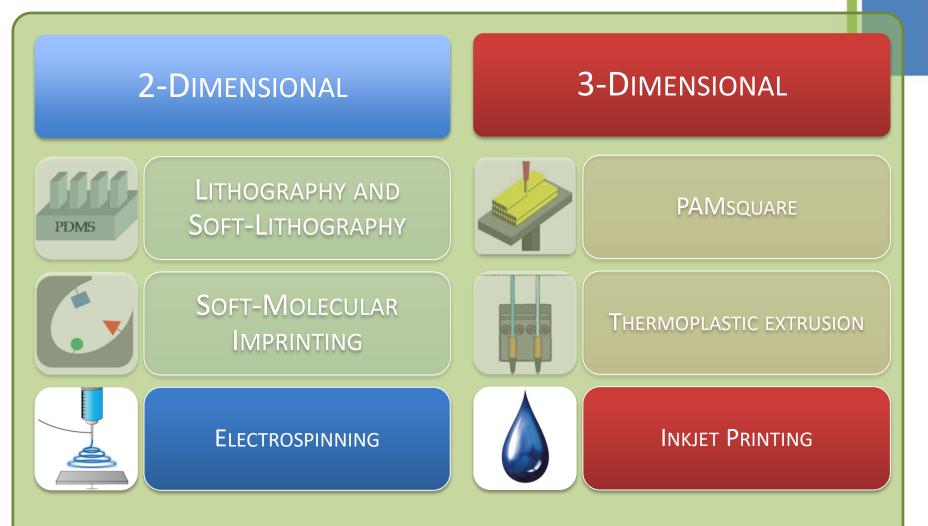
# Cell penetration into the scaffold

• RT4P6D2T at day5



Hoechst 33258 (Sigma Aldrich) was used as nuclear counterstain

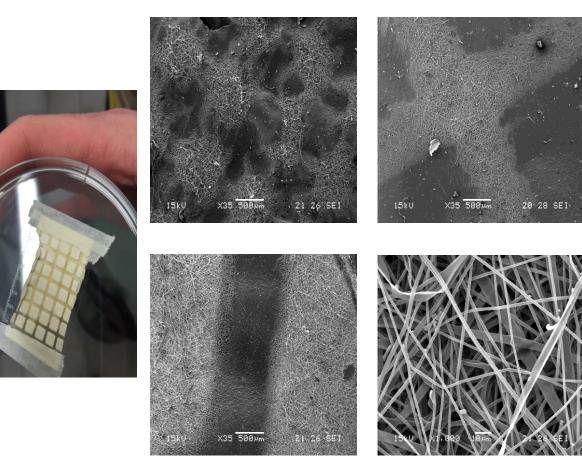
# **Multimaterial processing**



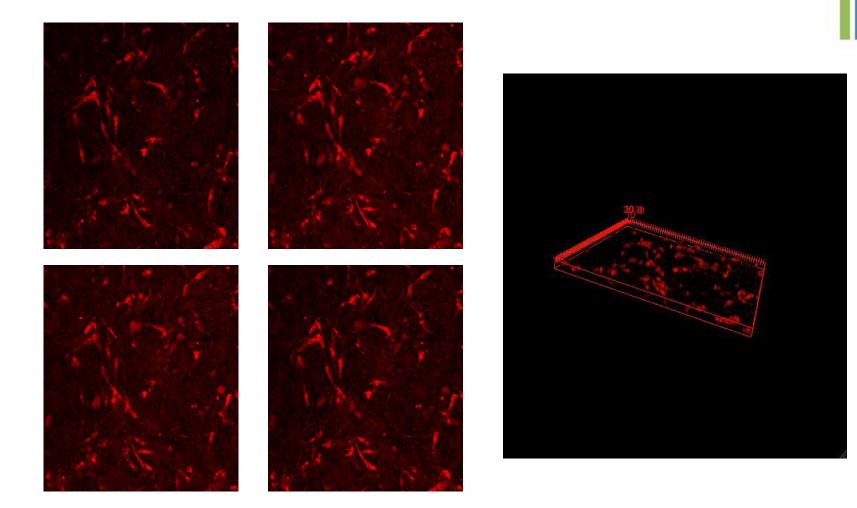
COMBINATION OF 2D AND 3D TECHNOLOGIES

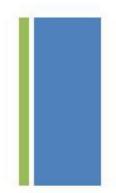
# Multiscale and multimaterial scaffold

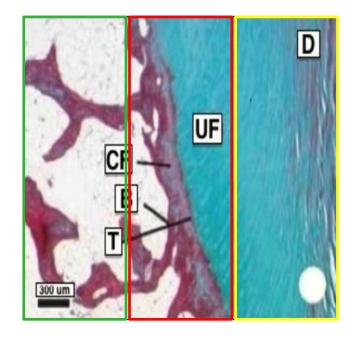
- Electrospinning and inkjet printing
- Introducing micro features on to nanofibers



# Multiscale and multimaterial scaffold





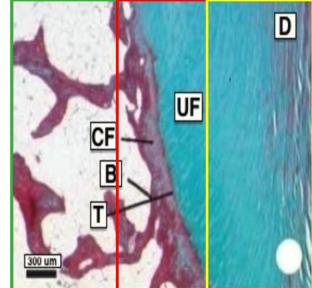


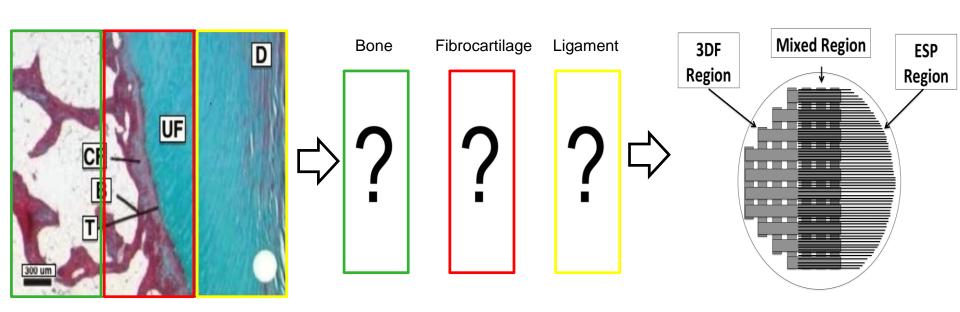
## **BONE LIGAMENT INTERFACE**

Criscenti G. et al. *Triphasic scaffolds for the regeneration of the bone-ligament interface*. Biofabrication. 2016 Jan 29;8(1):015009.

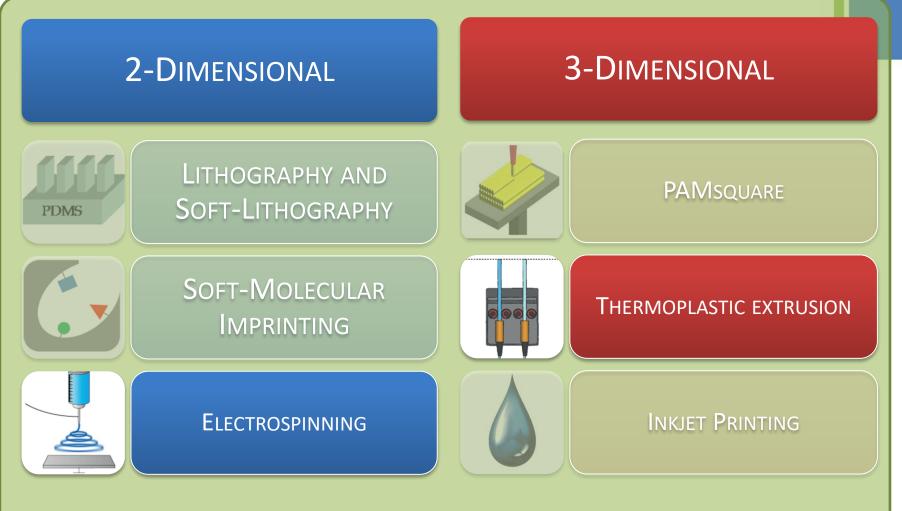
### **Bone-ligament interface**

- Enthesis:
  - also know as "insertion" or "attachment" site, or "osteotendinous" or "osteoligamentous" junction is the region where a tendon, ligament or joint capsule attaches to bone
- Fibrocartilagious enthesis
  - three different regions at the bone-tendon interface:
    - 1. Dense fibrous connective tissue (D)
    - 2. Uncalcified / calcified fibrocartilage(UF/CF)
    - 3. Bone (B)
  - Gradient of topological, chemical and mechanical properties

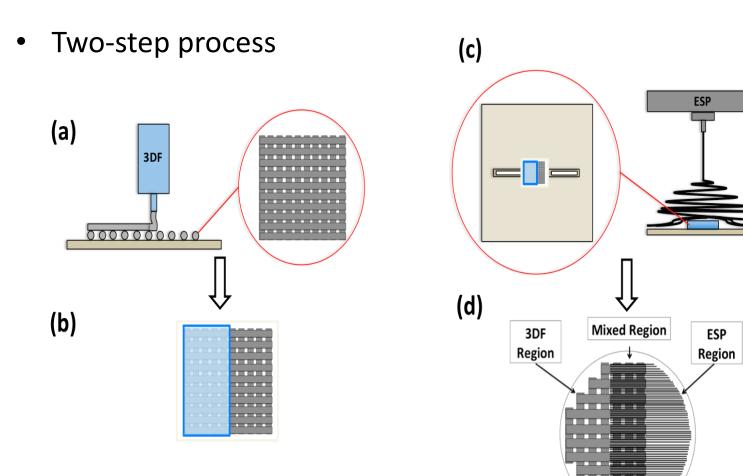


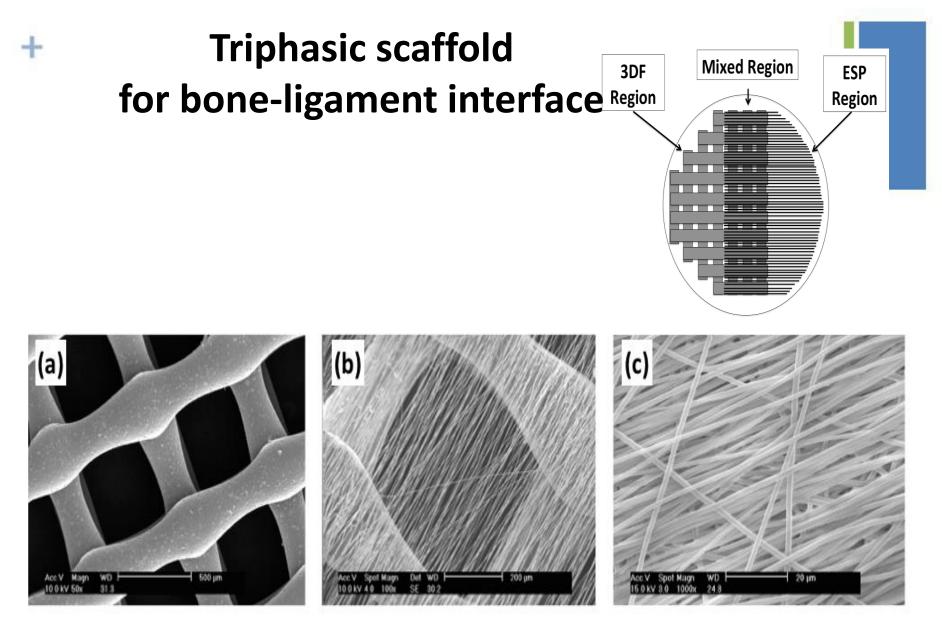


# **Multimaterial processing**



COMBINATION OF 2D AND 3D TECHNOLOGIES

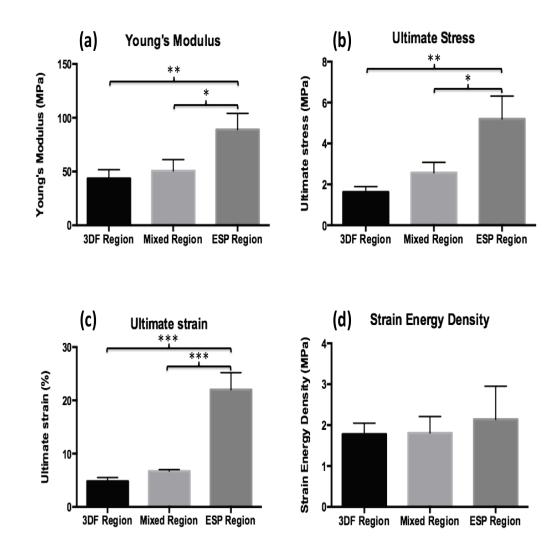




 $P = 77 \pm 1.7\%$ 

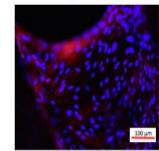
 $P = 68.9 \pm 3.1\%$ 

 $P = 95.9 \pm 1.6\%$ 

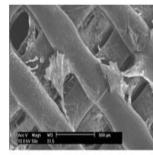


- hMSCs are an easily available cell source at the implantation site in orthopaedic applications
- hMSCs were homogeneously distributed on the entire scaffold and at the interface areas
- In the ESP mesh cells are well spread, whereas on the 3DF region they connect the fibers by bridging the pores.

DAPI/Phalloidin



SEM

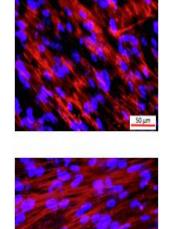


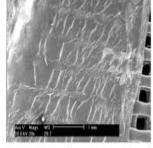
Mixed Region

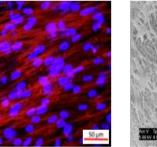
ESP

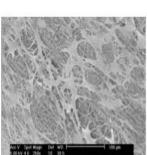
Region

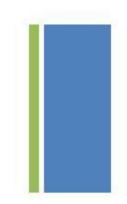
3DF Region

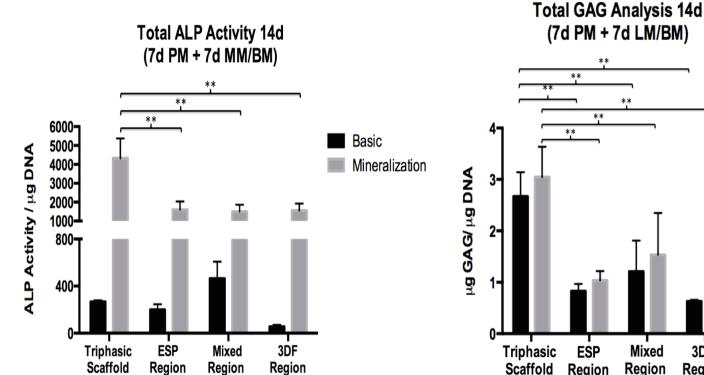




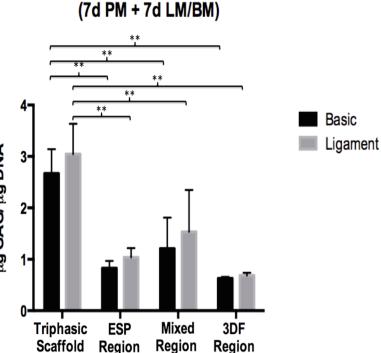




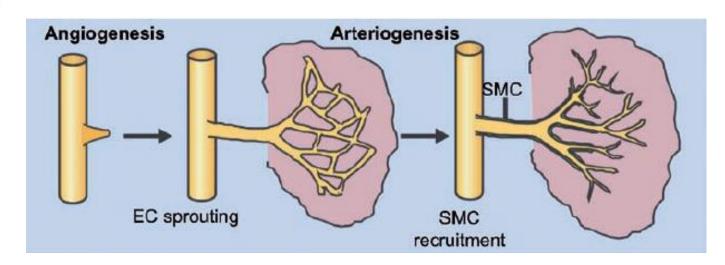




Total ALP activity after 7 day is PM and other 7 days in BM/MM. Controls were represented by scaffolds composed by only one region, thus being only eletrospun, 3DF and mixed structures.



Total GAGs after 7 day is PM and other 7 days in BM/LM. Controls were represented by scaffolds composed by only one region, thus being only electrospun, 3DF and mixed structures.



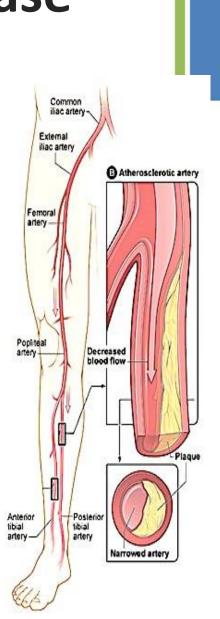
### STIMULATING REPARATIVE ANGIOGENESIS FOR PERIPEHRAL ARTERY DISEASES

Carrabba et al.

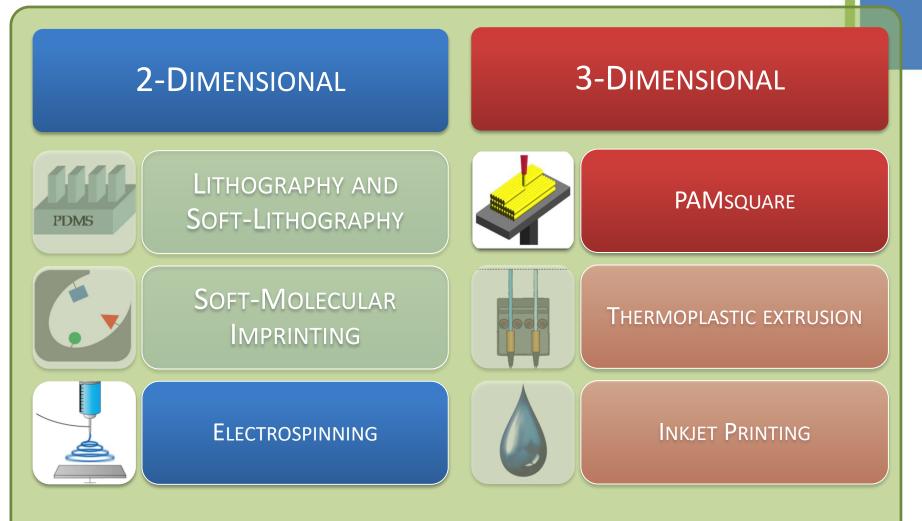
Design, fabrication and perivascular implantation of bioactive scaffolds engineered with human adventitial progenitor cells for stimulation of arteriogenesis in peripheral ischemia. Biofabrication. 2016 Mar 24;8(1):015020.

# **Peripheral artery disease**

- Incidence over 50 years of:
  - 1 in 5 man
  - 1 in 8 woman
- Critical Limb Ischemia
- Traditional medical approach:
  - Drugs
  - Surgical angioplasty
- Tissue Engineering: Design and development of a scaffold able to stimulate reparative angiogenesis in a mouse model of peripheral ischemia



# **Multimaterial processing**

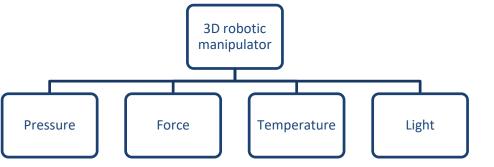


COMBINATION OF 2D AND 3D TECHNOLOGIES



- Modular CAD/CAM system
- A 3-axes robotic manipulator:
  - position ±50 mm;
  - velocity 0-15 mm/s;
  - resolution 1 μm;
  - different extrusion modules;
  - layer-by-layer processing.





Tirella A, De Maria C, Criscenti G, Vozzi G, Ahluwalia A. The PAM<sup>2</sup> system: a multilevel approach for fabrication of complex three-dimensional microstructures. Rapid Prototyping J 2012;18(4):5-5



# PAM<sup>2</sup>

#### Polyester structures

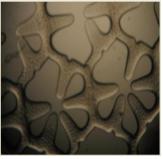


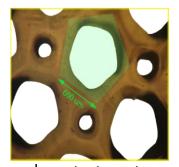


#### Natural polymer hydrogel structures



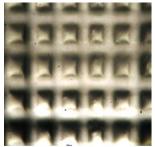
(self assembling polypeptide gels)



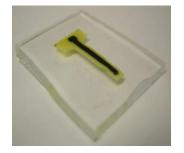


Laser ablation dry and wet structures









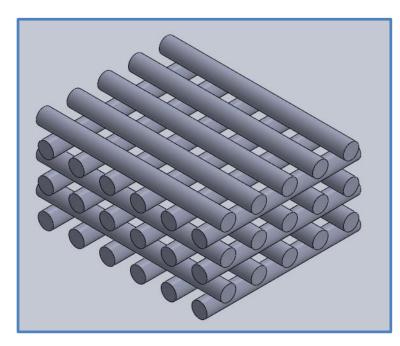
Polymeric actuators (condutive and dielectric ink)

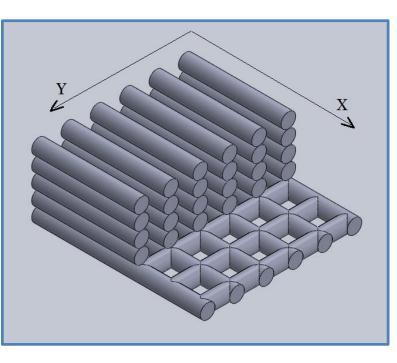
Gel-in-gel printing





# **Polymer structures**





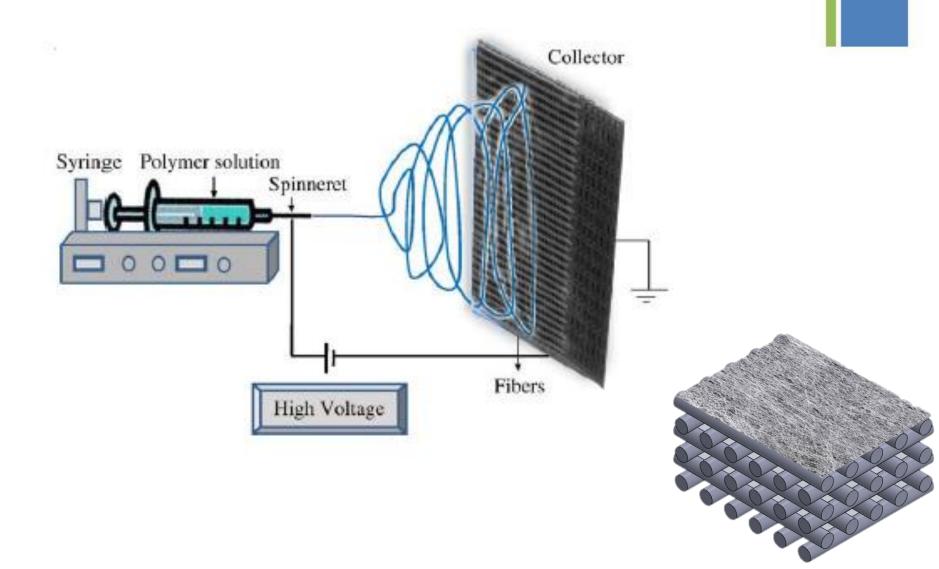
#### Woodpile structure

- PCL 10% w/v in chloroform
- Glass needle (⊗90 µm)
- Extrusion pressure 8kPa
- Deposition plate velocity 9 mm/s

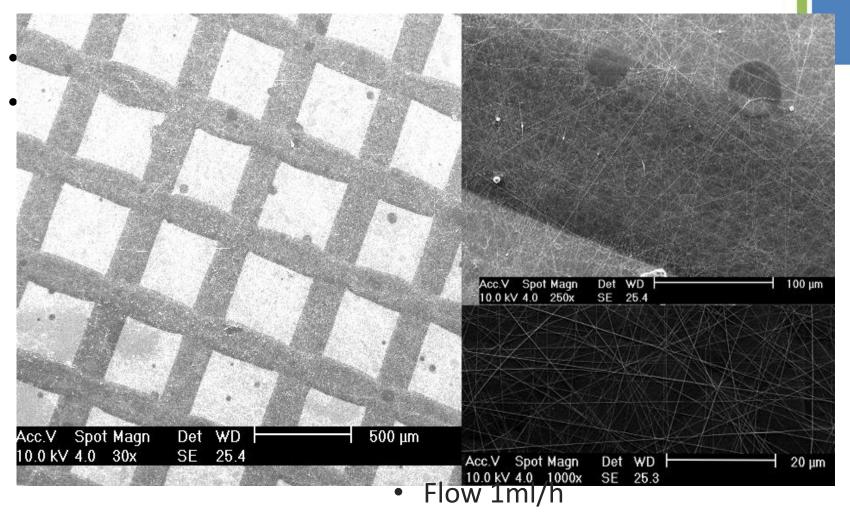
#### **Channel structure**

- 6 layers
- Total height 70±5µm

# **Electrospinning enhanced PAM<sup>2</sup>**



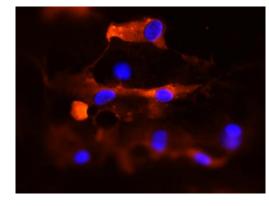
# **Electrospinning enhanced PAM<sup>2</sup>**

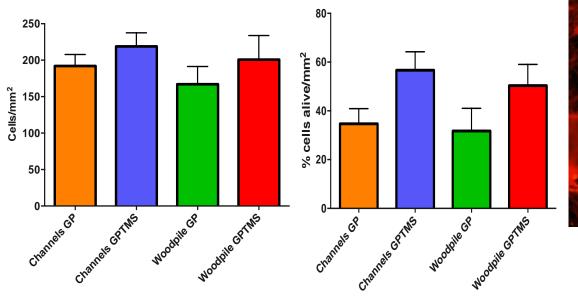


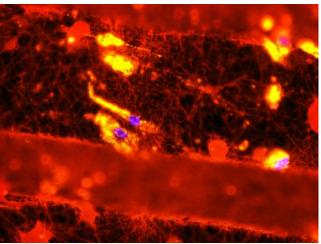
• Time of spinning 12 min

# In vitro assays

- **SVP** (saphenous vein pericytes) from **human** donors
- 10000 cells/well in 250 μl of complete media

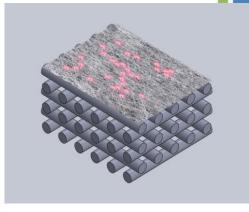


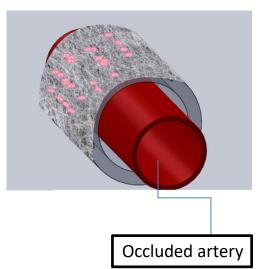




# In-vivo assays

- Channel structures crosslinked with GPTMS
- 3 groups of CD1 mice subject to Limb Ischemia at femoral artery:
  - scaffold implatation
  - scaffold, seeded with SVP, implantation
  - control
- End point 3 weeks





#### Laser doppler Area of scaffold implantation Foot scaffold lschemic to Contralateral Foot ontralateral Foo scaffold 1.0 1.0 cell scaffold ell scaffold ischem ia ischem ia 0.8 0.8 Blood flow ratio Blood flow ratio 0.6 0.6 υ 0.4 0.4 emic to 0.2 0.2 lsch 0.0 0.0 2 0 2 ო 0 ო

Before

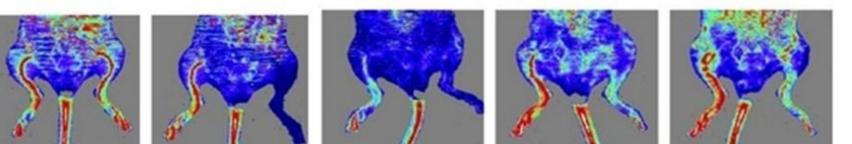
Scaffold



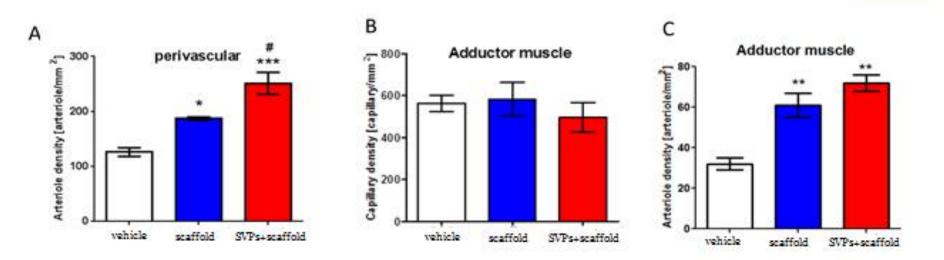
Day 7

Day 14

Day 21



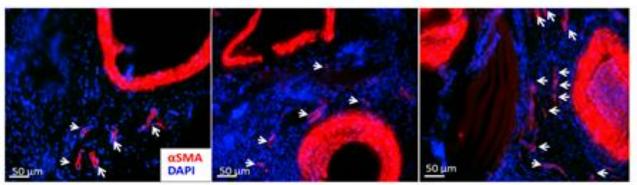
# Immunohistochemistry



scaffold

SVP +scaffold

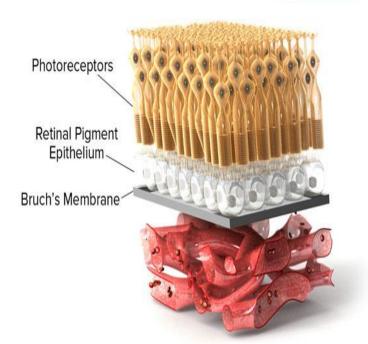
vehicle





#### Università di Pisa







MEDICAL

FACULDADE DE CIÊNCIAS MÉDICAS

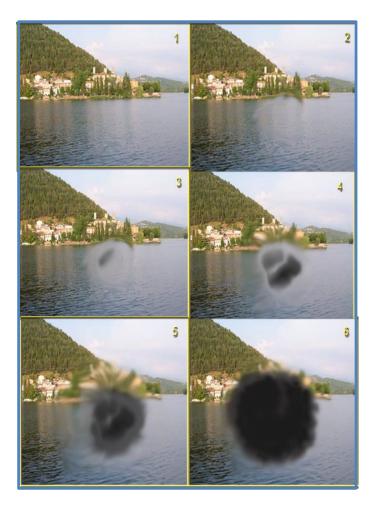
BIOMEMBRANE

### BIOENGINEERED IN VITRO MODEL OF RETINAL PIGMENT EPITHELIUM OF HUMAN EYE

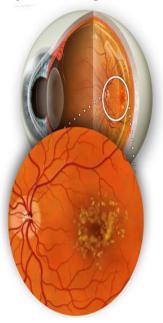


# Background

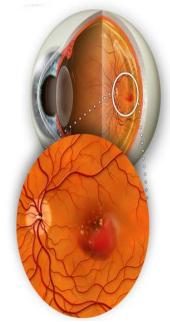
• Age-related macular degeneration



**Dry Macular Degeneration** 



#### Wet Macular Degeneration

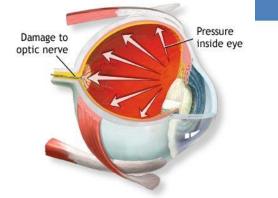


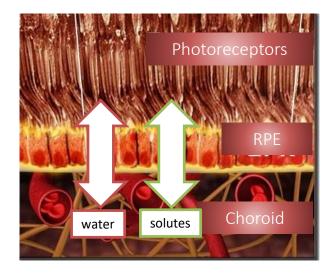
#### **Multimaterial processing 2-DIMENSIONAL 3-DIMENSIONAL** LITHOGRAPHY AND PAMsquare **SOFT-LITHOGRAPHY** PDMS SOFT-MOLECULAR THERMOPLASTIC EXTRUSION **I**MPRINTING **ELECTROSPINNING** INKJET PRINTING

COMBINATION OF 2D AND 3D TECHNOLOGIES

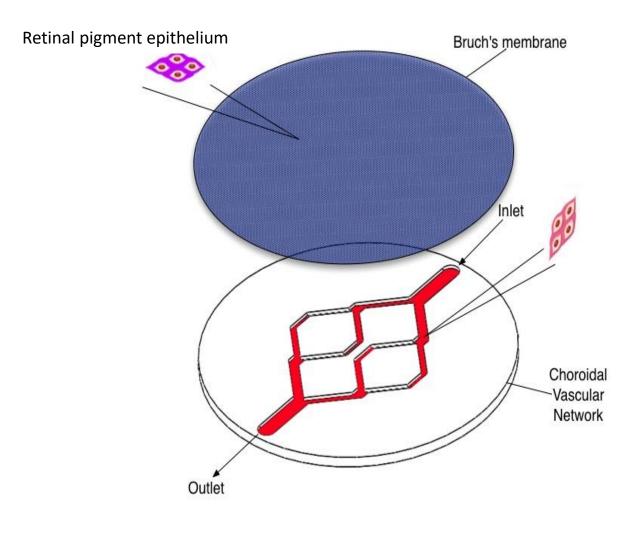
### **Bruch's membrane characteristics**

- Structural role
  - Mechanical resistance, agaist intraocular pressure
  - Elastic modulus 7-19 MPa
  - No changes during AMD
- Transport role
  - Convective transport (hydraulic resistance)
  - Diffusion driven process
  - Changes during AMD (in vitro model of the pathology)
- Electrospun meshes are a good model of Bruch's membrane





# Objective



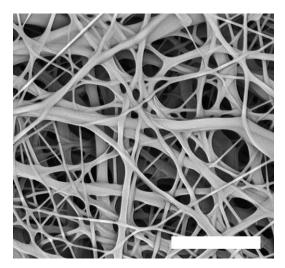




### Electrospun mat analysis

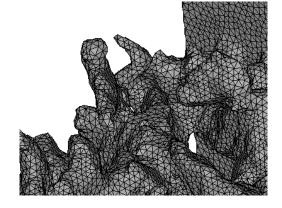
Realistic representation of the membrane structure was obtained through micro-computed tomography ( $\mu$ CT) (scan resolution 0.57  $\mu$ m) and SEM

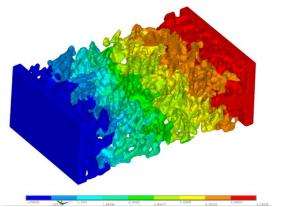


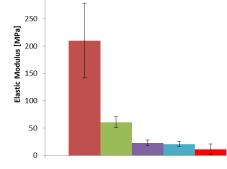


300



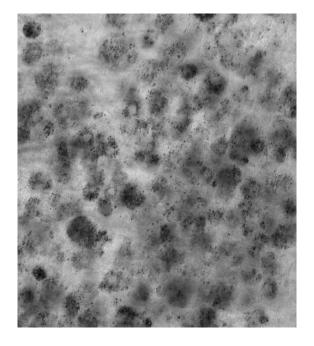


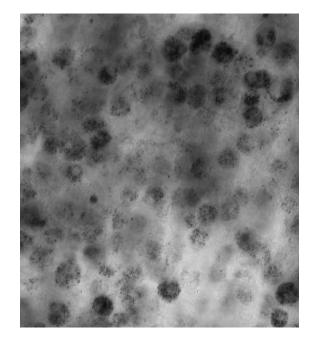




- Electrospun PLGA structures
  Electrospun gelatin type 1
  Electrospun gelatin type 2
- Electrospun gelatin type 3
- Bruch's Membrane

### **Culture hESc-RPE**





In vivo

In vitro

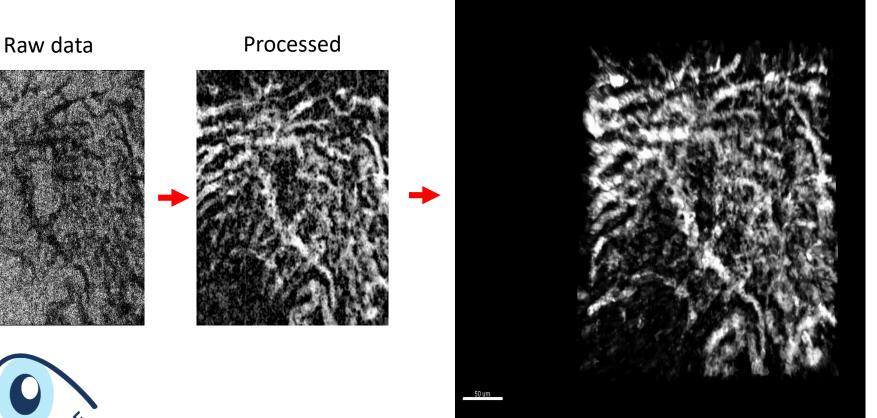




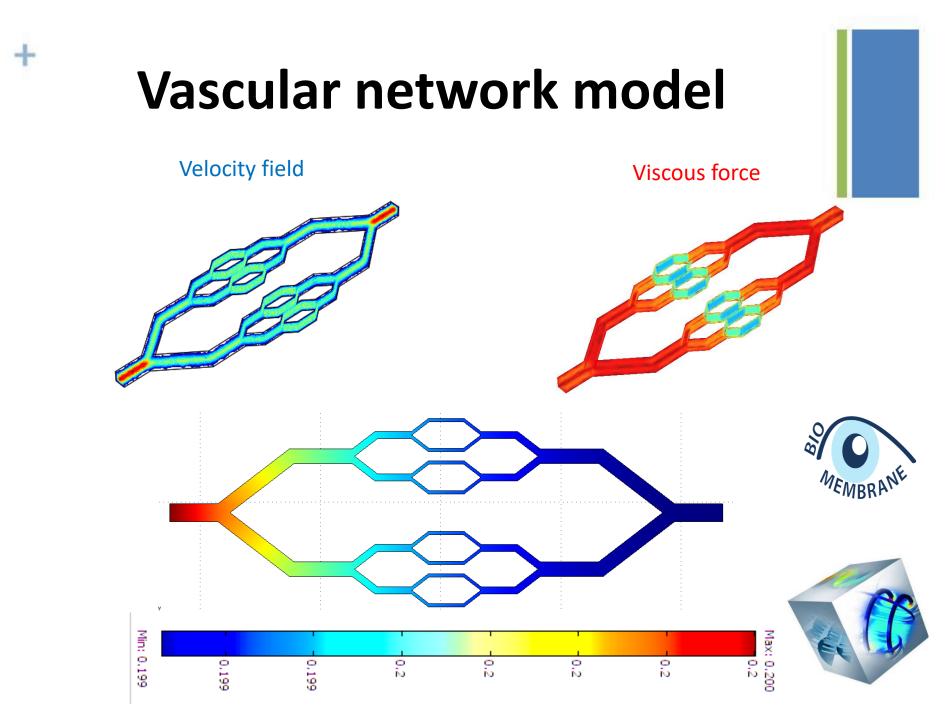
### **3D PROCESSING**



#### 3D reconstruction +







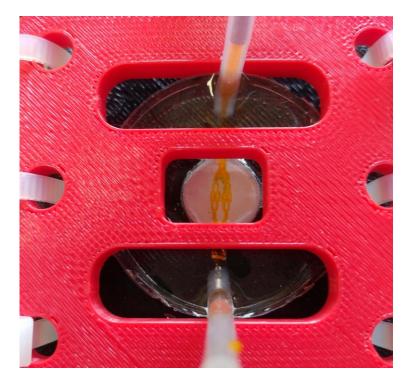
# **Mimicking blood vessels**

#### 3D model realised with Stereolithographic Printer Formlabs Form2





# **Mimicking blood vessels**













### Thanks for your attention!

#### **Biofabrication Group**



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